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51 **ABSTRACT**

52 **Introduction:** Longitudinal analyses of participants with a history of first-time lateral ankle
53 sprain are lacking. This investigation combined measures of inter-joint coordination and
54 stabilometry to evaluate static unipedal stance with eyes-open (condition 1) and eyes-closed
55 (condition 2) in a group of participants with chronic ankle instability compared to ankle
56 sprain ‘copers’ (both recruited 12-months after sustaining an acute first-time lateral ankle
57 sprain) and a group of non-injured controls.

58 **Methods:** Twenty-eight participants with chronic ankle instability, forty-two ankle sprain
59 ‘copers’ and twenty non-injured controls completed three 20-second single-limb stance trials
60 in conditions 1 and 2. An adjusted coefficient of multiple determination statistic was used to
61 compare stance limb 3-dimensional kinematic data for similarity in the aim of establishing
62 patterns of inter-joint coordination. The fractal dimension of the stance limb center of
63 pressure path was also calculated.

64 **Results:** Between-group analyses revealed that participants with instability displayed notable
65 increases in ankle-hip linked coordination compared to both copers (0.52 [1.05] vs -0.28 [0.9]
66 $p = 0.007$) and controls (0.52 [1.05] vs -0.63 [0.64] $p = 0.006$) in condition 1 and to controls
67 (0.62 [1.92] vs 0.1 [1.0] in condition 2.. Participants with instability also exhibited a decrease
68 in the fractal dimension of the center-of-pressure path during condition 2 compared to both
69 controls and copers. **Conclusion:** Participants with chronic ankle instability present with a
70 hip-dominant strategy of eyes-open and eyes-closed static unipedal stance. This coincided
71 with reduced complexity of the stance-limb center of pressure path in the eyes-closed
72 condition only.

73 **Key words:** ankle joint [MeSH]; biomechanical phenomena [MeSH]; kinematics [MeSH];
74 kinetics [MeSH]; postural balance [MeSH]

75

76 **INTRODUCTION**

77 Lateral ankle sprain (LAS) injury pervades a variety of activities, with between 0.88 [CI
78 95%: 0.73 – 1.02] and 7 [CI 95%: 6.82 – 7.18] injury events occurring per 1,000 exposures,
79 depending on the activity type (11). The prevalence of this injury in a wide range of sports
80 and activities is further complicated by its capacity to deteriorate into an array of chronic
81 sequelae and injury recurrence, collectively termed “chronic ankle instability (CAI)”(15-17),
82 which has been linked to limitations in future physical activity participation (1).

83 Although CAI is considered a multifaceted condition with a range of consequences, persistent
84 deficits in single-limb stance (SLS) postural control strategies are well established in
85 individuals with CAI (18, 25, 36), and may be consequent upon a potential change in neural
86 signalling following the initial ankle joint trauma (14). This theory has since been tested in
87 previous studies comparing individuals with a history of LAS to uninjured controls (13, 35,
88 37), with a new hypothesis emerging whereby the long-term outcome following LAS is
89 dependent upon the success or failure of the newly adopted post-LAS postural control
90 strategies (33, 34). This has yet to be confirmed however, as there is currently an absence of
91 longitudinal investigations which prospectively track the restoration or degradation of
92 postural control strategies after an initial LAS.

93 More recently, ankle sprain ‘copers’, who have a history of LAS and experience a restoration
94 of pre-injury levels of function in the year following initial injury (15, 33), have been
95 compared to individuals with CAI during SLS (36); this is considered to provide a stronger,
96 more relevant comparison in laying the foundation for longitudinal analyses and the
97 development of clinical outcome models for the CAI paradigm (33). Recently published
98 material from our laboratory was developed according to this paradigm: individuals with an
99 acute, first-time LAS were evaluated in comparison to a non-injured control group during
100 eyes-open and eyes-closed SLS using kinematic and kinetic measures of joint position and

101 platform stabilometry respectively (7). A follow-up analysis of these same individuals 6-
102 months following the initial assessment revealed a hip-dominant postural control strategy
103 prevailing during the prescribed tasks of SLS, again in comparison to non-injured controls
104 (9). In this latter investigation, an adjusted coefficient of multiple determination (ACMD)
105 statistic was utilised to evaluate waveform similarity between lower extremity 3-D joint
106 angular displacements in the determination of inter-joint ‘coupling’ strategies during 20
107 seconds of eyes-open and eyes-closed SLS (9). We believe novel insight was gained by
108 combining these laboratory measures: the increase in observed coupling between sagittal
109 plane hip and frontal plane ankle motion in LAS participants underpinned a hypothesis that
110 these individuals adopt a hip-dominant strategy in the maintenance of single-limb postural
111 control, perhaps to compensate for a dysfunctional ankle joint (9). This theory is in agreement
112 with the model of human postural control proposed by Nashner and McCollum, in which an
113 ‘ankle strategy’ is appropriated to the fine tuning of static postural control, and a ‘hip
114 strategy’ is employed to tackle more substantial postural control disturbances (28); the LAS
115 group in the aforementioned studies were considered to have reduced capacity to utilise their
116 ankle strategy, thus adopting the more proximal hip strategy in its place (7, 9).

117 The measure of platform stabilometry employed in the aforementioned investigations from
118 our laboratory was the fractal dimension (FD) of the center of pressure (COP) path. The FD
119 is a unit-less measure that conceptualises the complexity of the COP path using a value
120 between 1 (a straight line or low complexity) and 2 (a convoluted line or high
121 complexity)(23). In addition to a hip-dominant kinematical strategy, LAS participants were
122 also shown to display a bilaterally reduced FD of the COP path during eyes-closed SLS
123 within 2 weeks of incurring their initial injury (7), and on their involved limb only 6 months
124 following their initial sprain (9). This was interpreted as a reduced ability to utilise the
125 available base of support on removal of visual afferents (6, 7, 9).

126 The current study is a continuation of those previously described and forms part of a larger
127 longitudinal analysis of the LAS cohort. Specifically, we sought to complete the 12-month
128 follow-up of the individuals we previously alluded to who completed the 2-week and 6-
129 month evaluations, thus allowing for participant segregation as CAI or ankle sprain “coper”
130 status. Kinematic and stabilometric measures were combined to compare stance limb inter-
131 joint coordination and COP path complexity during eyes-open and eyes-closed SLS between
132 individuals with CAI, ankle sprain “copers” and a separately recruited non-injured control
133 group of participants. We hypothesised that individuals with CAI would exhibit the same hip-
134 dominant coupling strategies for completing eyes-open and eyes-closed SLS which were
135 documented 6-months previously, , whereas “coper” and control participants would not due
136 to a superior capacity to employ an ankle-based balance strategy in isolation. Furthermore,
137 we hypothesised that during eyes-closed SLS CAI participants would exhibit poorer postural
138 control ability, as evidenced by a reduced FD of the COP path.

139

140 **METHODS**

141 **Participants**

142 As part of the larger longitudinal study conducted in our laboratory, eighty-two individuals
143 presenting with a first-time acute LAS were recruited from a University-affiliated hospital
144 emergency department. All LAS participants were provided with the same basic advice on
145 applying ice and compression on discharge from the hospital ED: they were each encouraged
146 to weight-bear and walk within the limits of pain. Whether participants sought additional
147 formal medical healthcare services for council or rehabilitation of their LAS was recorded on
148 arrival to the testing laboratory but not controlled as part of the current study.

149 These individuals were required to attend three test sessions and complete a number of
150 movement tasks within 2-weeks of sustaining their initial injury, with further follow-up at 6

151 months and 12 months. Testing procedures for these participants in the acute phase of their
152 injury has previously been reported (6, 8, 10). A total of seventy-one of the original eighty-
153 two participants returned for the third test session (i.e. 12 month follow-up); the current
154 investigation relates to the data collected for these individuals at this time-point. An
155 additional convenience group of twenty participants with no prior history of LAS were also
156 recruited from the hospital catchment area population using posters and flyers to act as a
157 control group. Participant characteristics for the individuals included in the current analysis
158 are presented in Table 1. The following exclusion criteria were utilised for both limbs (where
159 applicable) at the time of recruitment: (1) no previous history of ankle sprain injury
160 (excluding the initial acute LAS episode for the CAI and copers groups); (2) no other severe
161 lower extremity injury in the last 6 months; (3) no history of ankle fracture; (4) no previous
162 history of major lower limb surgery; (5) no history of neurological disease, vestibular or
163 visual disturbance or any other pathology that would impair their motor performance.
164 Participants provided written informed consent, and the study was approved by the
165 University Human Research Ethics Committee.

166 LAS participants' designation as CAI or copers status was completed according to recently
167 published guidelines (15). Self-reported ankle instability was confirmed with the Cumberland
168 Ankle Instability Tool (15); individuals with a score of <24 were designated as having CAI
169 while "copers" were designated with a score of ≥ 24 , to avoid the potential for false positives
170 in this group (39). Additionally, to be designated as a copers, participants must have returned
171 to pre-injury levels of activity and function (36). Finally, the activities of daily living and
172 sports subscales of the Foot and Ankle Ability Measure (FAAMadl and FAAMsport) were
173 utilised as a means to evaluate general self-reported foot and ankle function (15). All
174 participants completed the CAIT and subscales of the FAAM on arrival to the testing
175 laboratory.

176 Based on these criteria, twenty-eight of the LAS participants were designated as having CAI,
177 and forty-two as “copers” (Table 1). One ‘coper’ participant was excluded because he did not
178 return to pre-injury levels of activity participation.

179

180 Protocol

181 Collection methods for this study have been previously documented (9). Briefly, following
182 the collection of anthropometric measures required for the calculation of internal joint centres
183 of the lower extremity joints, each participant was instrumented with the Codamotion
184 bilateral lower limb gait set-up according to the manufacturer guidelines (Charnwood
185 Dynamics Ltd, Leicestershire, UK). A neutral stance trial was used to align the subject with
186 the laboratory coordinate system and to function as a reference position for subsequent
187 kinematic analysis (40). Participants then performed three, 20 second trials of quiet SLS
188 barefoot on a force plate with their eyes-open on both limbs, each separated by a 30 second
189 rest period. Following another 2 minute rest period, participants then attempted to complete
190 three 20 second SLS trials with their eyes-closed. Participants were required to complete a
191 minimum of three practice trials on each limb for each condition prior to data acquisition (6,
192 21). Participants who were unable to complete a full trial of unilateral stance after five
193 attempts on the relevant limb were not included in the analysis for that limb. The test order
194 between legs was randomized. For both conditions of the SLS task, participants were
195 instructed to stand as still as possible with their hands resting on their iliac crests while
196 adopting a postural orientation most natural to them; the position of the non-stance limb was
197 not dictated in the sagittal plane as part of experimental procedures. Trials were deemed
198 invalid if the subject lifted their hands off their iliac crests, placed their non-stance limb on
199 the support surface, moved their non-stance hip into a position > 30 degrees abduction,
200 adducted their non-stance limb against their stance limb for support or if the foot placement

201 assumed by the participants relative to the support surface changed in any way over the
202 course of a trial. In addition a trial was deemed as failed in the eyes-closed condition if the
203 subject opened their eyes at any point.

204

205 Kinematic and Kinetic Data Processing

206 Three Codamotion cx1 units were used to acquire data on 3-D angular displacements at the
207 hip, knee and ankle joints for both limbs during the SLS tasks. Two AMTI (Watertown, MA)
208 walkway embedded force plates were used to acquire kinetic data. Kinematic and kinetic data
209 acquisition was made at 100 Hz. The Codamotion CX1 units were time synchronized with
210 the force plates. Kinematic and COP data were analysed using the Codamotion software and
211 then converted to Microsoft Excel file format. Temporal data were set with the number of
212 output samples per trial at 2000 + 1 in the data-export option of the Codamotion software,
213 which represented the complete unilateral stance trial as 100%, for averaging and further
214 analysis.

215 Pairwise comparison of 3-D temporal angular displacement waveforms for the hip and ankle
216 joints of the stance limb were made using the ACMD statistic (22) to determine the similarity
217 of a given pair of waveforms during both conditions of SLS. The pairing of ankle and hip
218 motion was completed in three dimensions, with nine resultant ACMD values for each
219 individual SLS trial. The mean ACMD from three trials of unilateral stance was used as a
220 representative ACMD for each participant for the eyes-open and eyes-closed conditions
221 separately, with subsequent calculation of group (CAI; coper; control) means. ACMD values
222 ranged from 0 (no similarity) to 1 (two identical curves) (22).

223 The kinetic data of interest was the COP, the location of the vertical reaction vector on the
224 surface of a force-plate) path (30). COP data acquired from trials of the unilateral stance were
225 used to compute FD of the COP path using an algorithm previously published and described

226 by Prieto et al (30). FD was calculated based on the 20 second interval for each SLS trial,
227 and averaged across the three trials for each participant on each limb and grouped
228 accordingly. The COP time series were passed through a fourth-order zero phase Butterworth
229 low-pass digital filter with a 5-Hz cut-off frequency(38).

230

231 Data Analysis and Statistics

232 For both LAS groups (CAI and coper), the limb injured at the time of recruitment was
233 labelled as “involved” and the non-injured limb as “uninvolved”. With regards to the
234 control group, limbs were randomly assigned as “involved” and “uninvolved” in all cases.
235 For all outcomes, we calculated mean (SD) scores for the involved and uninvolved limbs of
236 the CAI, coper and control groups.

237 A principal component analysis (PCA) was performed to reduce the dimensionality of the
238 kinematic data. Specifically, the nine ‘latent’ variables of inter-joint coordination were
239 reduced into significant components. This was performed separately for the eyes-open and
240 eyes-closed conditions. Preliminary analyses (scree test and parallel analysis) informed our
241 decision to retain three components for the eyes-open condition and two components for the
242 eyes-closed condition.

243 To test our hypothesis that the CAI group would display hip-dominant strategies of inter-joint
244 coordination , the components derived from the ACMD ‘latent’ variables were compared
245 between groups using a 2-way MANOVA for each condition (eyes-open and eyes-closed).
246 The independent variables were group (CAI; coper; control) and limb (involved; uninvolved).
247 The dependent variables were the three extracted components for the eyes-open condition and
248 the two extracted components for the eyes-closed condition. Preliminary assumption testing
249 was conducted to check for normality, linearity, univariate and multivariate outliers,
250 homogeneity of variance-covariance matrices, and multicollinearity with no serious

251 violations noted. An alpha-level of $p < 0.05$ was used to determine significant differences for
252 each analysis (19). Post-hoc comparisons were completed using a Tukey HSD test where
253 appropriate. The significance level for post-hoc analyses was set with a bonferroni adjusted
254 alpha of $p < 0.017$ for the eyes-open condition ($0.05/3$ components) and $p < 0.025$ for the
255 eyes-closed condition ($0.05/2$ components)(20).

256 In order to test our hypothesis that the CAI group would display reduced COP path trajectory
257 FD during the SLS task compared to copers and controls, a two-way between-groups analysis
258 of variance was conducted separately for each condition (eyes-open and eyes-closed). The
259 independent variables were group (CAI; coper; control) and limb (involved; uninvolved). The
260 dependent variable was FD of the COP path. The significance level for this analysis was set a
261 priori at $p < 0.05$. Post-hoc comparisons were completed using a Tukey HSD test where
262 appropriate. The significance level for post-hoc analyses was set at $p < 0.05$ for both
263 conditions.

264 All data were analyzed using Predictive Analytics Software (Version 18, SPSS Inc., Chicago,
265 IL, USA).

266

267 RESULTS

268 All participants completed the eyes-open SLS task on both limbs. Thirty-six percent of CAI
269 participants (10 of 28), 76% of copers (33 of 42) and 85% of controls (17 of 20) completed
270 the SLS task with their eyes-closed on both their 'involved' and 'uninvolved' limbs.

271 Regarding inter-joint coordination, there was a statistically significant main effect for group
272 in the eyes-open [$F(3,322) = 2.585, p = 0.018; \text{Wilks' Lambda} = 0.91$] and eyes-closed [F
273 ($3,220) = 3.58, p = 0.008; \text{Wilks' Lambda} = 0.88$] conditions. When the results of the
274 dependent variables were considered separately, the only components to reach statistical
275 significance at the bonferroni adjusted alpha levels were components 3 (which loaded heavily

276 on the inter-joint coordination between sagittal plane hip and frontal plane ankle motion, and
277 sagittal plane hip and transverse plane ankle motion) in the eyes-open condition [$F(2,321) =$
278 $6.508, p = 0.002, \eta_p^2 = 0.074]$ and 2 (which loaded heavily on the inter-joint coordination
279 between sagittal plane hip motion and ankle motion in all three dimensions, and frontal plane
280 hip motion and sagittal plane ankle motion) in the eyes-closed condition [$F(2,219) = 4.125, p$
281 $= 0.019, \eta_p^2 = 0.069]$. Post-hoc analysis and inspection of the mean scores revealed that CAI
282 participants exhibited lower mean scores for component 3 in the eyes-open condition, most
283 notably on their involved limb ($M = -0.52, SD = 1.05$) compared to both copers ($M = 0.28,$
284 $SD = 0.9, p = 0.007$) and controls ($M = 0.63, SD = 0.64, p = 0.006$). Due to the negative
285 correlation between component 3 and its latent variables, this represented an increase in
286 ankle-hip linked coordination. With regards to the eyes-closed condition, post-hoc analyses
287 revealed that CAI participants exhibited greater mean scores for component 2 compared to
288 controls only ($p = 0.024$). This was evident on both their involved (CAI: $M = 0.62, SD =$
289 $1.92; Control = 0.1, SD = 1.0$) and uninvolved (CAI: $M = 0.07, SD = 1.19; Control = -0.34,$
290 $SD = 0.66$) limbs. Due to the positive correlation between this component and its latent
291 variables, this too represented an increase in ankle-hip linked coordination.

292 Descriptive statistics for the ‘latent’ ACMD variables for the CAI, coper and control groups
293 prior to PCA are presented in Table 3. Pattern and structure matrices for the PCA relative to
294 the eyes-open and eyes-closed conditions are presented in Table 4.

295 Regarding the kinetic variables of interest, there was a statistically significant main effect for
296 group in the eyes-closed condition [$F(2,219) = 8.11, p = 0.001, \eta_p^2 = 0.12]$ only. Post-hoc
297 analysis and inspection of the mean scores revealed that CAI participants exhibited lower FD
298 of the COP path trajectory on their involved limb ($M = 1.78, SD = 0.11$) compared to both
299 copers ($M = 1.90, SD = 0.1, p = 0.045$) and controls ($M = 1.94, SD = 0.13, p < 0.001$).

300

301 In an exploratory analysis, the concurrent validity of four variables deemed ‘significantly
302 important’ (eyes-closed SLS task completion, component 3 in the eyes-open condition on the
303 involved limb, and both component 2 and the FD of the COP path on the involved limb in the
304 eyes-closed condition) in determining the extent of disability was established by calculating
305 their respective Pearson correlation coefficients to CAIT score. This was performed for LAS
306 participants only. The ability of each of these variables to determine outcome (CAI vs coper)
307 was then tested for sensitivity and specificity. A cut-off value of 0.7 was adopted for the C-
308 statistic in the sensitivity and specificity analyses.

309 There was no correlation between CAIT score and eyes-closed SLS task completion ($r =$
310 0.004 , $p = 0.97$), component 3 ($r = 0.109$, $p = 0.39$), component 2 ($r = 0.213$, $p = 0.19$) or FD
311 of the COP path ($r = 0.11$, $p = 0.39$).

312 However, eyes-closed SLS task completion was moderately predictive of outcome (CAI vs
313 coper), with a C-statistic of 0.71 ($p = 0.003$); the resultant prediction equation yielded a
314 sensitivity of 0.64 and a specificity of 0.78, with a positive likelihood ratio of 2.93.

315 To explain these findings, post-hoc analysis using independent samples t-tests were
316 performed to compare the CAIT scores of the subgroups of CAI and coper participants who
317 succeeded and failed at the eyes-closed SLS task. The p-value for this post-hoc analysis was
318 set a priori with a bonferonni adjustment at $p < 0.025$. This analysis revealed that copers who
319 were able to complete the task actually had significantly greater disability than those who
320 couldn’t, and likewise for the CAI participants, thus explaining the capacity of task
321 completion to predict outcome (CAI or coper), despite the absence of a correlation to CAIT
322 score. The results of this post-hoc analysis for both sub-groups of CAI and coper participants
323 are presented in Table 2. None of the other variables (components 2 and 3, FD of the COP
324 path) were predictive of outcome based on the C-statistic.

325

326 **DISCUSSION**

327 The primary finding of this motion analysis investigation was that individuals with CAI
328 exhibit greater ‘coupling’ of hip and ankle motion compared to both ankle sprain “copers”
329 and non-injured controls during an SLS task. This increase in ankle-hip ‘coupling’ may
330 represent a compensatory strategy to accommodate what is now a chronically unstable ankle
331 in the CAI group (as determined using the CAIT). Furthermore, the CAI group also
332 demonstrated a reduced FD of the COP path on their involved limb compared to both
333 “copers” and controls in the eyes-closed condition of SLS. These findings are consistent with
334 those previously published on this group as a whole within two-weeks of their injury (7), and
335 6-months following (9). Therefore, it is possible that the abatement of a hip-dominant
336 postural control strategy may be conducive to superior outcome. The design of the current
337 study however means that this cannot be confirmed.

338 To our knowledge, this is the first documented evaluation of postural control in a first-time
339 LAS population exactly 12-months following initial injury using kinematical measures of
340 inter-joint coordination and platform stabilometry. The advantage of the experimental design
341 is that all LAS participants (CAI and copers) were recruited at the time of their first ankle
342 sprain injury, thereby securing the homogenous subgroups of ankle sprain outcome. As we
343 have alluded to, this study is part of a longitudinal analysis designed to develop an outcome
344 model for the predictors of instability following ankle sprain injury.

345 The use of “copers” provides a superior comparison group to individuals with CAI than non-
346 injured controls because copers have had the same exposure, but are not characterized by the
347 same symptom sequelae as those individuals who develop CAI (33). The addition of a non-
348 injured control group in this report has however allowed us to identify that, based on the
349 parameters utilised in the current investigation, LAS “copers” are no different to non-injured
350 controls in their postural control strategies for eyes-open and eyes-closed SLS. This is

351 evidenced by the absence of between-groups differences for copers and controls in this
352 analysis, which is in agreement with previous findings during a similar task protocol (31, 36).
353 It has recently been identified that this tripartite comparison between CAI, “coper” and
354 control participants is needed in the context of ankle sprain research(33). Indeed, there are
355 only a limited number of previous analyses which have evaluated movement patterns in these
356 groups (4, 5, 31, 36, 37) with fewer still providing an analysis of SLS postural control using
357 measures of platform stabilometry (31, 36). Wikstrom et al. (36) identified that ankle sprain
358 coper participants’ stance limb COP paths exhibits a lower velocity in both the antero-
359 posterior and the medio-lateral axes of the foot than individuals with CAI during a similar
360 task. Shields et al.(31), demonstrated that the standard deviation of the COP path and it’s
361 range were significantly lower in “copers” compared to subjects with CAI, a finding the
362 authors interpreted as being demonstrative of better postural control predictability.

363 The issue regarding the application of these ‘traditional measures’ of COP excursion which
364 quantify the length, area and velocity of the COP path, apart from their questionable
365 reliability (12), is that they have previously yielded inconsistent or even contradictory
366 findings in ankle sprain populations (26). By contrast, the FD measure utilised in the current
367 analysis is a reliable measure (12) which has previously been successful in characterising a
368 degeneration in stability of the postural control system in the transition from eyes-open to
369 eyes-closed stance (3). Furthermore, because we have adopted the FD calculation in
370 analysing the COP paths of these same participants during SLS within 2-weeks (7) of
371 incurring their initial injury and 6-months later (9), its use enables us to directly compare our
372 findings across time points relevant to the development of CAI or ankle sprain coper status.

373 Consistent with the investigations of these participants 2-weeks and 6-months following
374 injury occurrence (7, 9), the findings of the current study revealed that individuals with
375 poorer outcome (<24 on the CAIT in this study, ‘injured’ status in those previously

376 described), exhibit reduced FD of the COP path compared to individuals with superior
377 outcome (non-injured controls and “copers”), albeit in the eyes-closed condition only. This
378 was previously interpreted as a reduced ability to utilise the available base of support during
379 SLS, isolated to instances where the task condition dictated the removal of visual afferents
380 (6). Similarly, the CAI participants in the current study also exhibited greater ‘coupling’ of
381 hip-ankle joint coordination in the completion of eyes-closed SLS compared to controls, a
382 finding consistent with the acute (2-week) and injury “twilight” (6-month) data.

383 .
384 That a lower proportion of the CAI group were able to complete the balance task in the eyes-
385 closed condition prompted an exploratory analysis, whereby this dichotomous outcome and
386 the other group-defining variables (components 3, 2 and the FD of the COP path) were
387 separately correlated with CAIT score. Their capacity to predict outcome (CAI vs coper) was
388 also evaluated. While the group-defining variables exhibited no correlation with CAIT score,
389 and did not predict outcome, task completion was determined as predictive of CAI or coper
390 status. . The moderate specificity and sensitivity that an ability to complete eyes-closed SLS
391 had in predicting outcome, in the absence of a correlation to CAIT score, may be under-
392 lied by a disability ‘cut-off’; the correlation between CAIT score and task ability is probably not
393 linear, wherein it is possible that at a certain point, an individual’s ability to perform a
394 difficult balance task (such as eyes-closed SLS) deteriorates drastically. Individuals below
395 this cut-off have the potential to be equally likely to be unable to complete the task, whether
396 they have “more” or “less” disability. Future analyses are required to elucidate such ‘cut-offs’
397 however.

398 The apparent difficulty CAI participants had in completing eyes-closed SLS may represent an
399 impaired capacity to compensate and re-coordinate the available sensory afferents, or to rely
400 on the remaining somatosensory and vestibular afferents when visual ones have been

401 removed (24). It is generally accepted that there is redundancy of these three afferents in
402 maintaining SLS (29), whereby a selective priority is placed based on the availability of
403 reliable information (27). This allows the fully functioning somatosensory system to maintain
404 postural control and stability in the presence of altered afferent signals (24). However,
405 prescribing an eyes-closed constraint during the SLS task imposes somatosensory demands
406 beyond the capacity of even healthy individuals (as evidenced by the fact that 15% of
407 controls were unable to complete our eyes-closed task protocol), impairing their ability to
408 exploit available redundancies in the maintenance of static postural control (7). This
409 impairment is seemingly magnified in individuals with musculoskeletal injury on the basis of
410 the current findings, and in light of the evidence previously outlined of participants with a
411 recent history of ankle sprain (7, 9). Thus, a decay in somatosensory afferents, as may occur
412 with acute LAS injury and which is considered to contribute to instability persistence (14),
413 combined with loss of visual input, challenged the ability of the central nervous system to re-
414 coordinate the available information with an appropriated postural control response (13, 27)
415 in individuals with CAI. This then manifested in a deterioration of eyes-closed unilateral
416 standing postural control and stability in the CAI group, with less effective utilisation of the
417 supporting base on the involved limb (7). It is also plausible that the somatosensory
418 deterioration associated with CAI development manifested in a ‘hip-dominant’ compensatory
419 strategy as evidenced by the significantly greater ankle-hip coupling compared to both
420 “copers” and controls in the eyes-open condition, and compared to controls in the eyes-closed
421 condition. Whereas the ankle strategy of human postural control is more suited to subtle
422 corrections, the hip strategy is considered ideal for substantial disturbances of equilibrium
423 (24). Tropp (32) previously utilised kinematic measures of sway amplitude at the ankle, hip
424 and trunk to confirm the existence of these strategies. He also identified the impaired postural
425 control capacity of individuals with ankle instability in utilising their ankle strategies for SLS,

426 based on an increased number of postural corrections at the trunk required by this group (32).
427 In another kinematic analysis of participants with a history of ankle sprain during an SLS
428 task, Huurnink et al.(21) failed to identify differences in kinematic outcome measures (ankle
429 and hip angular velocities) between participants with and without a history of ankle sprain.
430 We believe the use of the ACMD statistic in the current study to have specifically identified
431 an increased reliance on the more proximal hip strategy in the CAI group, on the basis of the
432 greater waveform similarity between these joints. During normal control of SLS, the foot's
433 narrow base of support makes it necessary to employ the hip strategy in controlling
434 substantial medio-lateral disturbances of postural stability, while ankle movements may only
435 achieve fine-tuning of medio-lateral sway (2). The basis of CAI may be belied by an impaired
436 capacity to fulfil this medio-lateral fine-tuning, with subsequent transition to the more
437 proximal hip. Herein lies a significant limitation of the current analysis; these and any other
438 hypotheses regarding the neuromechanical predictors of CAI still unclear, although the
439 current study is part of a project designed to investigate this issue. Another significant
440 limitation of this analysis is that we were unable to experimentally control whether LAS
441 participants sought additional rehabilitation for their injury. However, to do so would have
442 been unethical, and no treatment data 'clusters' were evident during data management and
443 analysis.

444 The clinical implications of this study are two-fold: first, in light of the evidence presented on
445 these individuals during their 'recovery', it would seem that the capacity to perform static
446 postural control tasks will challenge the individual to perform subtle corrections with ankle
447 movements. A SLS task and derivations of such may therefore possess value in being part of
448 a rehabilitation programme. Based on previous evidence, we would recommend though that
449 the patient only progresses to such tasks when they are sufficiently able to complete them (6).

450 Second, the use of eyes-closed SLS as a clinical test to quantify disability and functional
451 capacity should be considered. There is further potential for future research to confirm this.
452 In conclusion, the results of the current study suggest that participants with CAI are separated
453 by ankle sprain copers and non-injured controls in their exhibition of a hip-dominant balance
454 strategy during a task of eyes-open and eyes-closed unilateral stance.

455

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460

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